Ischaemic heart disease (IHD) related mortality has been on the decline, although its prevalence has been on the rise since the late 1970s. One of the contributing factors to this decline has been improved diagnosis and therapeutic management. Every clinician seeks to answer four key questions while evaluating patients with suspected or known IHD: What is the global ventricular function? What is the regional ventricular function? Is the myocardium viable? What is the status of the coronary arteries? In the past decade cardiovascular magnetic resonance (CMR) imaging has emerged as an important clinical technique with the potential of answering all the pertinent questions in a single study. This has led to a significant increase in demand and utilisation of this modality. However, many clinicians are not well versed with this technology, its clinical utility, limitations and future prospects. With the increasing prevalence of IHD, CMR imaging is likely to be used more often in its diagnosis, prognostication and management. The review describes the basic principles and practical aspects of CMR imaging, and then discusses in detail the role of CMR in the diagnosis and management of IHD, its complications, and its utility in patients with acute myocardial infarction.

ABSTRACT

Ischaemic heart disease (IHD) is the most common cause of death in the UK, with one in five men and one in six women dying from the disease. Death rates from IHD in the UK have been declining since late 1970s, although its prevalence is on the rise. This fall in death rate could be attributed to a multitude of causes including changing lifestyle, environmental factors, and advancements in health care. Cardiovascular magnetic resonance (CMR) imaging is one such advancement in the field of health care, which has emerged as an important clinical technique in the diagnosis, therapeutics and prognostication of IHD.

In assessing a patient with IHD every clinician seeks to answer four key questions as shown in box 1. In the past, non-invasive imaging of IHD included chest radiography, echocardiography (echo), and nuclear cardiology. These different imaging modalities were used in conjunction with each other to answer these specific questions, which led to inadvertent delays in management and had significant financial implications. Clinical emphasis should be on better patient selection and initiation of appropriate treatment. This can be achieved by CMR, which over the last decade has emerged as a test with the potential of providing all the above information in a single study. CMR, with its higher spatial resolution and excellent soft tissue contrast, can also provide valuable information that may not be available from other diagnostic tools. This has led to its increased clinical demand and utilisation worldwide. However, many clinicians are not well versed with this technology, its clinical utility and limitations. We describe the basic principles and practical aspects of CMR imaging, and then discuss in detail the role of CMR in the diagnosis and management of IHD, its complications, and its utility in patients with acute myocardial infarction.

BASIC PRINCIPLES AND PRACTICAL ASPECTS OF CMR IMAGING

Magnetic resonance imaging (MRI) is dependent on the magnetic properties of the spinning hydrogen nuclei found within water and fat molecules. The scanner itself is a large magnet and when a patient enters it, the inherent spinning hydrogen nuclei align either along or against the magnetic field of the scanner. This alignment is then disturbed by an extrinsic radiofrequency pulse, which is then turned off, allowing nuclei to return back to their initial state of alignment. The latter leads to release of a radio signal that is used to create the final image.

CMR can acquire both static and live cine images. To prevent blurring of the image, ECG gating is used. Static images are preferentially acquired during diastole while cine images are acquired during the entire cardiac cycle. Different pulse sequences are used in CMR; these can be broadly classified into dark blood and bright blood sequences based on the colour of fast flowing blood. Dark blood sequences are good for anatomic delineation of blood vessel lumen and cardiac chambers. Bright blood sequences are used for live cine imaging of the heart. The standard protocol used for assessing IHD by CMR in our institution is shown in table 1. Images are acquired in standard planes that closely mimic the planes used in echocardiography and are shown in figure 1. The duration of CMR scan depends on the clinical question being answered and varies from 30 min to an hour. Patients are supine on the table and are asked to hold their breath (7–20 s) while images are being acquired. Arrhythmias and inability to hold breath adequately can lead to a suboptimal study.

MRI is safe and no long-term ill effects have been demonstrated. One of the most important safety issues for CMR is to avoid ferromagnetic substances near the scanner, as they can become projectiles. Metallic implants such as hip prostheses, prosthetic heart valves, coronary stents and sternal sutures are not a contraindication since these are not ferromagnetic. Care is required in patients with many cerebrovascular clips and

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specialist advice is needed for such patients. Patients with pacemakers, implantable cardioverter defibrillators (ICDs), retained permanent pacemaker leads and other electronic implants are currently not scanned.2

CMR IN THE DIAGNOSIS AND MANAGEMENT OF ISCHAEMIC HEART DISEASE

Pathophysiology of myocardial ischaemia
Myocardium may exist in different physiological states (table 2). The most precise definition of infarction, and therefore loss of viability, is that myocyte death must have occurred. The presence or absence of cell death can be established by microscopy or histological stains. However, this is not obviously practical in a clinical setting. Consequently, several less precise definitions of viability have been developed that are based on parameters that are more easily measured in patients.6 7 All ischaemic events before cell death are, at least in principle, reversible by re-establishment of an adequate blood supply. Therefore, it is important to differentiate between viable and non-viable states as revascularisation of the former improves left ventricular (LV) function and long term survival, while revascularisation of non-viable myocardium is associated with increased mortality.8 12 Subendocardium is most vulnerable from ischaemia and, depending on the extent and duration of ischaemia, myocardial necrosis can extend transmurally towards the epicardium in a distribution corresponding to the perfusion territory of the diseased vessel.13 Viable myocardium may be hypo-contractile in the setting of chronic myocardial hyperperfusion or acute myocardial ischaemia. Hibernating and stunned myocardium are terms used to describe this phenomenon of viable but dysfunctional myocardium. Stunned myocardium is usually seen in the setting of acute infarction and shows improved recovery in the long term.

Table 1 Standard cardiovascular magnetic resonance (CMR) protocol used for assessing ischaemic heart disease (IHD) with their specific clinical utility

<table>
<thead>
<tr>
<th>IHD assessment CMR protocol sequences</th>
<th>Clinical utility</th>
</tr>
</thead>
<tbody>
<tr>
<td>Static dark blood images of the thorax (HASTE sequence)</td>
<td>Demonstrate anatomy and extra cardiac abnormalities</td>
</tr>
<tr>
<td>Bright blood cine images in the following planes</td>
<td>Assess global and regional ventricular function.</td>
</tr>
<tr>
<td>2 Chamber (vertical long axis)</td>
<td>Demonstrate valvular dysfunction</td>
</tr>
<tr>
<td>4 Chamber (horizontal long axis)</td>
<td>Detect ventricular thrombus</td>
</tr>
<tr>
<td>3 Chamber</td>
<td></td>
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<tr>
<td>Short axis (from base to apex of heart)</td>
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<td>Left ventricular outflow tract (LVOT)</td>
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<td>Myocardial stress imaging: Adenosine stress/rest perfusion or Dobutamine stress wall motion analysis</td>
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<td>Post-gadolinium enhancement static images Early Flow studies in breath hold and free breathing</td>
<td>Detect ventricular thrombus and microvascular obstruction Valvular functional analysis</td>
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<tr>
<td>Late Coronary artery imaging</td>
<td>Assess origins and proximal course</td>
</tr>
</tbody>
</table>

Figure 1 Standard planes of image acquisition on cardiovascular magnetic resonance (CMR) imaging. (A) Two chamber. (B) Three chamber. (C) Four chamber. (D) Left ventricular outflow tract (LVOT). (E) Right ventricular outflow tract (RVOT). (F) Sino-atrial (SA) base. (G) SA mid ventricle. (F) SA apical ventricle. AA, ascending aorta; LA, left atrium; LV, left ventricle; PA, pulmonary artery; RA, right atrium; RV, right ventricle.
Clinical indications
The clinical indications for performing CMR in patients suspected or known to have IHD are outlined in box 2. As mentioned previously, in clinical practice it is not practical to assess myocardial viability by microscopy and histology. Information acquired from CMR can help in making this distinction between viable and non-viable myocardium non-invasively. The clinical indications of CMR in IHD are primarily aimed at answering the four critical questions outlined in box 1. Answers to these questions not only help in reaching the correct diagnosis but also help in streamlining the management and assessing the prognosis.

Regional ventricular function assessment by CMR
Regional ventricular function assessment by CMR includes regional wall motion abnormality (RWMA) and LV myocardial thickening. Regional functional analysis is vital as it can recognise areas of transmural chronic infarction which is characterised by severe myocardial thinning and lack of wall thickening in systole (figure 5). Multiple studies have shown that myocardial segments with an end diastolic wall thickness (EDWT) <6 mm most likely represent transmural scar formation, and contractile function will not improve after revascularisation. However, an EDWT >6 mm does not necessarily imply functional recovery after revascularisation.

On CMR, RWMA is analysed on bright blood cine images acquired in multiple planes. For standardised assessment and documentation of myocardial analysis the 17-segment model of the American Heart Association is universally used (figure 4). A normal contractile pattern consists of endocardial inward movement and systolic wall thickening. RWMA is graded as: hypokinetic, when endocardial inward movement and systolic wall thickening are present but decreased; akinetic, when there is lack of endocardial inward movement and absent systolic wall thickening; and dyskinetic, when there is paradoxical systolic endocardial outward movement and/or systolic wall thinning.

RWMA on CMR can be assessed both qualitatively (visually) and quantitatively. One of the quantitative analytic methods is myocardial tissue tagging where radiofrequency pulses are used to create regular dark bands (saturation bands) over the image. These bands form a diamond shape over the myocardium and will be distorted by myocardial contraction, while areas of akiinesia or hypokinesia will have no or minimal distortion.

Qualitative and quantitative RWMA analysis with CMR are both well validated. As mentioned earlier, an EDWT >6 mm on its own does not imply functional recovery after revascularisation and additional tests (stress and viability analysis) are required for predicting the outcome of these segments.

Myocardial viability analysis by CMR
Viable myocardium is characterised by the presence of living myocytes irrespective of contractile function or response to extrinsic stimuli. Hypocontractility in itself does not necessarily equate to non-viability and could be secondary to chronic myocardial hypoperfusion or acute myocardial ischaemia. Assessment of viability by CMR is based on demonstrating indirect signs of significant coronary artery disease, which include:

Myocardial contractile reserve by dobutamine stress study
Adequate myocardial perfusion on adenosine/dipyridamole stress study
Intact myocyte cell membrane on delayed enhancement imaging.

Myocardial contractile reserve by dobutamine stress study
Bright blood cine CMR performed during dobutamine infusion is a well-established technique for demonstrating ischaemia...
induced wall motion abnormality and may also be used to assess potential for contractile response to revascularisation in IHD. Dobutamine is a synthetic β₁ adrenergic catecholamine and has a positive inotropic effect. Dobutamine infusion leads to increased myocardial oxygen consumption which cannot be compensated by significantly occluded coronary arteries, leading to ischaemia and decreased contractility and thickening of the myocardium.

Dobutamine has a rapid onset of action and short half-life of about 120 s, allowing gradual drug titration. To improve sensitivity, patients are asked to stop taking β-blockers 24–48 h before the test. Most side effects of dobutamine are mild (anxiety, palpitations, chest tightness, etc) and resolve spontaneously after termination of stress. If symptoms persist, side effects can be reversed by administration of a short acting β-blocker. Severe complications (ventricular tachycardia, ventricular fibrillation and myocardial infarction) are rare and can be seen in up to 0.3% of patients receiving high dose of dobutamine. Contraindications to dobutamine stress testing include acute coronary syndrome, severe aortic stenosis, hypertrophic obstructive cardiomyopathy, uncontrolled hypertension/atrial fibrillation/heart failure, and known severe ventricular arrhythmias.

The study is performed by intravenous infusion of dobutamine in 3 min stages at incremental doses from 5–40 µg/kg/min under continuous monitoring of ECG, blood pressure (BP) and symptoms. If peak stress level, defined as target heart rate of [220–age] × 0.85, is not achieved then additional fractioned atropine doses of 0.25 mg every minute up to 1 mg can be given. Selected cine images in both short and long axis are acquired at rest and at every incremental stage of stress. Images at different stages can then be compared side by side for the onset of new regional wall motion abnormalities.

Images can be analysed both visually and quantitatively. For standardised assessment and documentation findings are reported as per the 17-segment model. Dysfunctional but viable myocardium (hibernating and stunned) will show improvement of systolic contraction and wall thickening at low dose dobutamine infusion (5–10 µg/kg/min). High dose dobutamine protocols (up to 40 µg/kg/min) are used to improve the sensitivity and to demonstrate the biphasic response: initial improvement of contractile function at low dose and worsening of contractile function at high dose, caused by stress induced ischaemia.

Reported sensitivity and specificity of dobutamine CMR in predicting functional recovery ranges from 50–82% and 81–90%, respectively. By using quantitative assessment methods the sensitivity and specificity can be as high as 89% and 93%, respectively. Dobutamine CMR is superior to stress echocardiography due to higher quality imaging and lack of dependence on adequate ultrasound windows. On the other hand, stress echocardiography is preferred by some clinicians in assessment of patients with concurrent mitral regurgitation or aortic stenosis. There is a low cardiovascular event rate when the dobutamine CMR is normal and a higher event rate in the presence of ischaemia.

Myocardial perfusion analysis by CMR

Myocardial perfusion analysis is achieved by obtaining a live movie of the transit of contrast medium with the blood during its initial transit through the LV myocardium—in other words, it demonstrates the first pass perfusion of the myocardium. First pass perfusion of the LV myocardium is analysed at both peak stress and at rest. These are compared with each other to assess stress induced perfusion defects and ischaemia.

Adenosine is the most commonly used pharmacological agent for stress perfusion analysis. Adenosine is a vasodilator that...
increases the myocardial blood flow by four- to fivefold down-stream of a normal coronary artery. In a severely diseased artery there is no such increase in flow, as the capillaries are already maximally dilated, leading to delayed delivery of contrast which is seen as an area of hypo-enhancement or darkness.

Commonly adenosine is infused intravenously at the rate of 140 μg/kg/min under continuous monitoring of blood pressure, ECG and symptoms. The available alternative agent is dipyridamole with a half-life of 30 min, compared to 10 s of adenosine, making it difficult to control effectively. Patients usually experience shortness of breath, chest tightness, palpitations and a drop in blood pressure that resolve spontaneously after stopping adenosine. Adenosine is to be avoided in patients with severe asthma, high degree atrioventricular (AV) block, significant valvular stenosis and patients on dipyridamole due to its potentiating effect.37

Adenosine is infused for at least 3 min to achieve peak vaso-dilatation. After this a bolus of gadolinium contrast agent (0.1 mmol/kg) is injected and the myocardium is imaged. Recurrent images are acquired at selected short and long axis planes on every heartbeat (for 50 beats) while patients are holding their breath. The infusion is then stopped and early post-gadolinium imaging performed to demonstrate microvascular obstruction, which is seen as areas of low signal in subendocardial distribution. Late gadolinium enhancement (LGE) imaging is then performed, and is discussed in detail later. About 20 min after the completion of the adenosine infusion, myocardial rest perfusion is performed in a similar way to the stress study but without adenosine infusion. Images can be assessed qualitatively by visual inspection or semi-quantitatively. Visual analysis is adequate in a clinical setting and characterises perfusion defects as reversible when present only at stress, and fixed when present in both stress and rest (figure 5).

CMR is now an attractive alternative to single photon emission computed tomography (SPECT) and positron emission

Figure 4 Seventeen segment model used for standard nomenclature, depicting the left ventricle basal, mid, apical cavity and apex distribution.

Figure 5 SA LV mid (A, C) and apical cavity (B, D) views in peak stress (A, B) and rest (C, D). Note significant subendocardial stress induced perfusion defect (arrow) in the antero septal wall which completely resolves at rest. LV, left ventricle; RV, right ventricle.
tomography (PET) myocardial perfusion imaging. This is due to improved subendocardial resolution, cost effectiveness, and lack of ionising radiation in CMR. Multiple trials comparing CMR with SPECT, PET and/or coronary angiography have shown positive results, with sensitivity and specificity of CMR in detecting perfusion defects of 87–90% and 85%, respectively. CMR perfusion has also established its role in imaging patients with cardiac syndrome X, wherein one has typical anginal symptoms, abnormal exercise test, but a normal coronary angiography. It is possible to show a subendocardial perfusion defect associated with intense chest pain by CMR in patients with syndrome X.

**LGE imaging**

Late or delayed phase enhancement imaging after gadolinium injection is a simple technique that allows detection of myocardial infarction (MI) and assessment of myocardial viability. This is perhaps the most widely used and validated CMR technique for assessing viability. Evidence from many previous studies has shown that delayed hyperenhancement is observed in regions of myocardial irreversible injury.

Gadolinium is an extracellular CMR contrast agent and does not traverse intact cell membranes. The normal myocardium is tightly packed with muscle with minimal extracellular space and has a uniform low signal. In areas of infarction, the extracellular compartment is expanded and washout of contrast from these areas is slow. This leads to a higher concentration of contrast which is seen as a bright signal. With its high spatial resolution (1.2×1.2 mm) it is possible to determine the transmural distribution of MI on CMR (figure 6). Gadolinium has a good general safety profile, but needs to be used with caution in patients with impaired renal function and is contraindicated in patients with a glomerular filtration rate (GFR) <50 ml/min/1.75 m² as it can induce nephrogenic systemic fibrosis (NSF). NSF is typically seen in patients with end stage renal disease and most are on regular dialysis treatment. It begins with subacute swelling of distal parts of the extremities followed during subsequent weeks by severe skin induration and sometimes anatomical extension. Skin induration may be aggressive and associated with constant pain while in some cases it can lead to serious disability requiring use of a wheelchair. NSF can also extend to involve several organs such as the liver, lungs and heart which may explain suspected increased mortality in these patients.

There is no universal consensus about the pathophysiology of NSF, but the working hypothesis is that in patients with end stage renal failure there is delayed or no excretion of free gadolinium, which is extremely toxic. This free gadolinium is thought to deposit in the tissues and lead to NSF.

LGE imaging is typically performed 5–10 min after injection of gadolinium and static images are acquired in long axis and short axis plane covering the whole myocardium. To improve sensitivity and specificity of detecting hyperenhancement the signal from adjoining normal myocardium is nulled by using a special inversion recovery sequence.

Abnormal enhancement caused by IHD should be limited to a vascular territory and subendocardium is the most vulnerable part of the myocardium. LGE by CMR is highly sensitive and can identify abnormal enhancement even when wall motion and perfusion by SPECT are normal. LGE by CMR has been tested for predicting viability, and when the transmural extent of infarction/hyperenhancement is <50% the likelihood of functional recovery in acute MI or with bypass surgery is good.

Identification of infarcted myocardium is also important because it provides a substrate for ventricular tachyarrhythmias. The technique is reproducible, superior to SPECT, and excellent when directly compared with PET.

Myocardial hyperenhancement outlines areas of myocardial fibrosis, which is a final common pathway for myocardial injury. Therefore it can be seen in other conditions affecting the myocardium, although the pattern of hyperenhancement is different. In contrast to subendocardial/transmural enhancement seen in IHD, patients with sarcoidosis and dilated cardiomyopathy tend to have mid wall enhancement, while patients with hypertrophic cardiomyopathy have patchy enhancement not confined to a vascular territory. Myocarditis on the other hand can have either epicardial or mid myocardial hyperenhancement (figure 7).

Comprehensive evaluation of viability by CMR is performed differently at different centres. LGE imaging tends to form the core of viability analysis and can be used on its own or in combination with either dobutamine or adenosine stress analysis. The former has the advantage of being quick, safe and not requiring specialist supervision. However, addition of one of the stress protocols is thought to improve the specificity of the viability analysis. The choice between the two stress protocols is dependent on user experience, patient factors (for example, severe asthma is a contraindication for adenosine), and local guidelines. In our centre, apart from LGE, we reserve the use of adenosine stress study in patients with suspected or known single vessel coronary artery disease, whereas double or triple vessel disease assessment is performed by dobutamine stress study. This is to prevent false negative first pass perfusion analysis secondary to multivessel balanced myocardial ischaemia.

**Coronary artery imaging and CMR**

CMR at present has a limited role in coronary artery imaging. This is mainly due to the small size, tortuosity and constant movement of the coronary arteries with every heartbeat and breath. Multidetector computed tomography (MDCT) remains the forerunner in non-invasive assessment of coronary vessels because of its superior spatial resolution (0.5–0.6 mm) and shorter breath hold. Emphasis has therefore been on depicting the functional impact of coronary artery disease in the form of regional wall motion abnormality or perfusion defects. Currently coronary artery imaging by CMR can be performed in
both breath-hold and free breathing states. The latter uses navigator technology where artefact secondary to breathing is nulled by tracking the movement of the diaphragm during image acquisition.

In clinical practice CMR coronary artery imaging is currently limited to assessing the anomalous origin and proximal course of the vessels (figure 8). This is usually performed after coronary angiography to ensure that the proximal portion does not have a malignant course between the pulmonary artery and the aorta. There have been further promising studies assessing the role of CMR in imaging coronary artery disease and have shown a 81% negative predictive value in excluding multivessel proximal disease. However, assessment of severity of stenosis and distal vessels remains a technological challenge.

CMR imaging of acute MI
CMR allows complete and accurate assessment of LV status in patients with acute MI, and contrast enhanced imaging visualises total infarct size and microvascular obstruction (MVO) in vivo. Despite successful recanalisation of infarct related artery by percutaneous coronary intervention, perfusion of the ischaemic myocardium is not completely restored in up to 30% of patients due to MVO. This is known to be a predictor of adverse events, higher incidence of ventricular remodelling, congestive heart failure, and death. The role of CMR in acute MI is currently limited to monitor patients after acute myocardial infarction in clinical trials. Because of its capacity to assess global/regional ventricular function, size and transmurality of infarction and MVO in one single examination, CMR is expected to become an important imaging modality in the evaluation of patients with acute MI.

SUMMARY
CMR on its own allows comprehensive assessment of patients with IHD. Patients with poor LV function have a worse prognosis and CMR is the current gold standard imaging modality for assessment of ventricular function. Viability analysis is vital as revascularisation of non-viable myocardium and medical management of viable myocardium are associated with poor outcome. CMR can accurately distinguish viable from non-viable myocardium and demonstrate subendocardial ischaemia even before there is perfusion abnormalities on SPECT. The current role of CMR in coronary artery imaging is CMR not only helps in accurate quantification of interventricular shunt but is also useful in surgical planning. Mitral valve incompetence is a known complication of IHD. Along with LV functional analysis, CMR can provide important data on the amount of mitral regurgitation which will also guide further management.

Key learning points
- With increasing prevalence of IHD there is increased demand and utilisation of CMR imaging in patients with IHD.
- CMR on its own allows comprehensive assessment of patients with IHD by providing accurate data on global and regional ventricular function.
- CMR can accurately distinguish viable from non-viable myocardium and can also demonstrate subendocardial ischaemia at an early stage.
- CMR has a limited role in coronary artery imaging.
- CMR also helps in surgical planning and prognosticating patients with IHD.

Current research questions
- Improved myocardial perfusion analysis on 3 Tesla CMR scanners.
- Technological improvement in spatial resolution and ECG/respiratory gating to improve coronary artery imaging on CMR.
- Role of CMR in evaluation of syndrome X.
limited to assessment of the origin and proximal course of the vessels. From the available evidence and clinical practice, CMR might therefore be regarded as a ‘one stop shop’ for assessment of IHD.

**MANY CHOICE QUESTIONS (TRUE (T)/FALSE (F); ANSWERS AFTER REFERENCES)**

**Question 1:**
A. Ischaemic heart disease is the leading cause of death in UK
B. IHD related mortality is on the increase
C. Patients with permanent pacemakers cannot have CMR
D. CMR contrast agent contains gadolinium
E. Dobutamine is a negative inotropic agent

**Question 2:**
A. Left ventricular volumes and ejection fraction calculated by CMR are not reliable
B. There is a good likelihood of functional recovery in a myocardium which has <50% subendocardial infarction on CMR
C. Subendocardium is the most viable part of myocardium to ischaemia
D. LGE is only seen in patients with myocardial infarction
E. NSF is usually seen in patients with good renal function

**Question 3:**
A. Hypocontractile myocardium is always non-viable
B. CMR is the imaging modality of choice for non-invasive assessment of coronary artery disease
C. CMR does not involve any radiation exposure to the patient
D. Adenosine used in myocardial stress test is a vasoconstrictor
E. Stunned myocardium is seen in the setting of acute myocardial infarction

**Question 4:**
A. Assessment of myocardial mass is a recognised indication for CMR
B. Depressed LV systolic function is a marker of poor prognosis
C. For standardised analysis and documentation, the 17-segment model of the American Heart Association is universally utilised
D. Regional wall motion abnormality on CMR can be analysed both quantitatively and qualitatively
E. Dobutamine has a short half life of 120 min

**Question 5:**
A. Viable myocardium will show improvement in contractility at low dose dobutamine stress
B. Adenosine has a half life of 10 s
C. Adenosine is contraindicated in patients with severe asthma
D. Coronary artery imaging by CMR can be performed under free breathing
E. ECG gating is not necessary in CMR

**Competing interests** None.

**REFERENCES**


**ANSWERS**

1. **A (T); B (F); C (T); D (T); E (F)**

2. **A (F); B (T); C (T); D (F); E (F)**

3. **A (F); B (F); C (T); D (F); E (T)**

4. **A (T); B (T); C (F); D (T); E (F)**

5. **A (T); B (T); C (T); D (F); E (F)**

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Ischaemic heart disease assessment by cardiovascular magnetic resonance imaging

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